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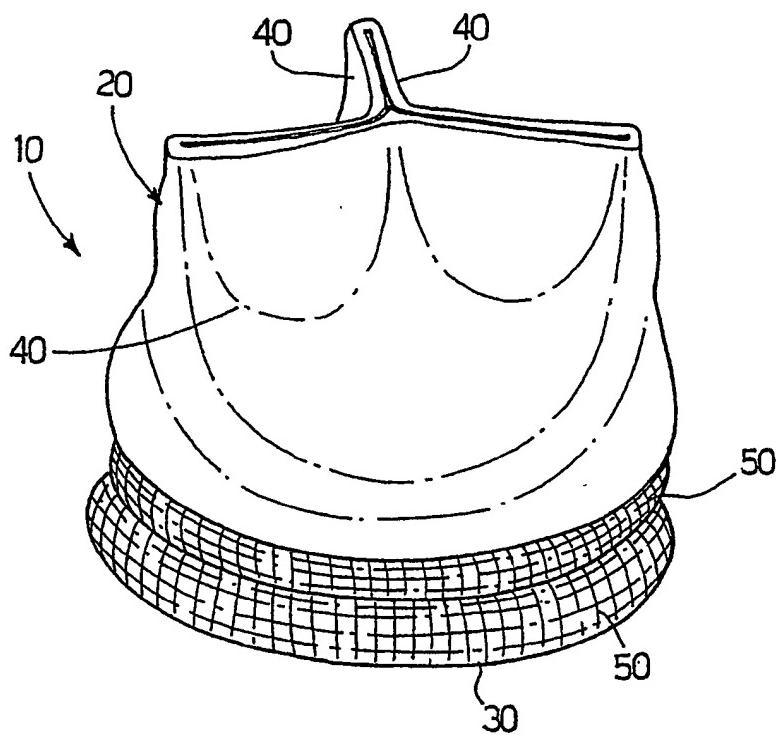
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(54) Title: A PROSTHETIC VALVE APPARATUS, IN PARTICULAR FOR CARDIAC APPLICATIONS



(57) Abstract: A prosthetic valve apparatus (10), in particular for cardiac applications. The apparatus (10) comprises a valve prosthesis (20) fastened to a suture ring (30). The apparatus (10) further provides for the valve prosthesis (20) to be fastened to the suture ring (30) by means of a plurality of magnets (21d, 30b) which provide a magnetic attraction between the two components.

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For two-letter codes and other abbreviations, refer to the "Guidance Notes on Codes and Abbreviations" appearing at the beginning of each regular issue of the PCT Gazette.

A PROSTHETIC VALVE APPARATUS, IN PARTICULAR FOR CARDIAC APPLICATIONS

5 TECHNICAL FIELD

The present invention relates to the field of medical prosthetic apparatuses in general, and in particular to a prosthetic valve apparatus able to be implanted in a body district of the organism of humans 10 or of mammals in general.

BACKGROUND ART

The scope of the invention falls within the field of medicine, and in particular that of heart surgery, and it is aimed at the treatment of congenital or 15 acquired valve pathologies for which it is indicated to replace with prosthesis one or more natural heart valves irreversibly compromised by pathological processes with different etiology.

The replacement of one or more heart valves with 20 prostheses has long been a commonly accepted procedure. The surgery procedure normally entails the use of extra-body circulation, able to allow access to the cardiac cavities with the heart stopped and bloodless.

However, in spite of the advances made so far 25 within the field of heart surgery, it can be stated that this type of operation is not free of possible complications able to induce morbidity or even mortality of the operated patients.

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According to the general classification, currently two main categories of prosthetic substitutes of cardiac valves are clinically available:

- (1) mechanical valve prostheses; and
5 (2) biological valve prostheses.

The specialist scientific literature describes in detail the types of prostheses, the indications pertaining to their selection, the surgical technique for their implant, possible complications and results.

10 However, it seems useful, to understand the subject and the innovative aspects included in the present invention, to provide a short foreword on the state of the art.

In the mechanical valve prostheses of the first
15 type, the blood flow that traverses them is controlled by one or more shutters constitute by metallic rigid bodies assembled in such a way as to be able to oscillate on a respective rigid metallic annular support.

20 Instead, in the second case, i.e. in the case of biological valve prostheses (the so-called "bioprostheses"), the blood flow is controlled by strips constituted by biological tissue assembled on a rigid support.

25 In bioprostheses, the tissue used is generally of animal origin (bovine pericardium or native strips of porcine heart valve) preventively treated chemically to make it immunologically inert and structurally stable.

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Among the biological tissues used for the construction of heart valves, a new biomaterial derived by corneal stroma of tuna has recently and advantageously been introduced with the aim of reducing 5 or eliminating the possibility of structural failure of the bioprostheses over time.

In all cases (mechanical and biological apparatuses) as a structural component of the valve is included a component (the so-called "suture ring") 10 assembled at the outer perimeter of the base of the prosthesis, able to house it and fasten it by means of suture stitches in orthotopic valve position instead of the previously excised native valve.

It is readily apparent that the presence of the 15 suture ring at the outer perimeter of the base of the valve prosthesis determines a significant reduction in the effective area of the valve orifice.

Moreover, it is evident that the support of the biological strips (the so-called "valve stent", or 20 simply "stent") also significantly limits the haemodynamic disengagement of the valve, causing a reduction in the useful area of opening of the prosthesis.

To make biological valve apparatuses anatomically 25 more similar to natural heart valves and to improve their haemodynamic disengagement, numerous structural improvements have been introduced over time, giving rise to the sub-category of biological valve prostheses

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without support (so-called "stentless valves") and with suture ring positioned at the level of the base of the valve and not at the level of the outer perimeter of the prosthesis.

5 These solutions have enabled to obtain biological heart valve prostheses with a greater effective area of the valve orifice than traditional biological valves provided with stents. In spite of the evident haemodynamic benefits provided by the use of stentless
10 biological valves, it is more difficult to implant this type of prosthesis than traditional biological valve prosthesis provided with stent and suture ring positioned at the outer perimeter of the stent.

This drawback is particularly reflected in the need
15 for prolonged operating times with the heart stopped and in extra-body circulation and in the possibility of an incorrect positioning of the prosthesis at important structures adjacent to the implant site.

An additional drawback of biological prostheses in
20 general, and of stentless ones in particular, is the impossibility of *in situ* orientation (i.e. after the implant), due to the absence of any system that allows the rotation of the valve prosthesis on the suture ring. This drawback is reflected in the absolute need to
25 determine the correct orientation of the prosthetic apparatus during the operation, before executing the suture of the valve ring at the anatomic implant site.

In regard to the durability of the valve prostheses

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over time, it can be stated that mechanical valve prostheses have a duration that is practically unlimited over time due to the materials of construction, for example metal alloys which may be coated with pyrolytic
5 carbon.

However, at the same time, mechanical valve prostheses have the disadvantage that the operated patient has to assume anti-coagulating and anti-aggregating thrombocytic drugs throughout his/her life,
10 in order to prevent very sever, and even lethal, episodes of thromboembolism due to the contact of the blood with the metallic prosthetic material.

While biological valve prostheses do not have require the administration of anti-coagulating drugs,
15 nonetheless have limited duration over time (from a few years in young patients, to a maximum of ten-fifteen years in older ones) due to the formation of calcium deposits within the valve strips, able to cause their structural failure.

20 The progressive deterioration of biological prostheses over time imposes a new surgical operation to replace the prosthesis with another valve prosthesis, entailing considerable operative risk in terms of morbidity and mortality of the operated patients.

25 In fact, in heart surgery it is not unusual to perform multiple interventions on the same patient after a time interval to replace deteriorated biological prostheses.

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Therefore, the problems normally encountered when using traditional biological valve prostheses can be summarised as follows:

- limited duration over time, with the consequent need to replace the prosthesis;
- effective area of the valve orifice (useful area for the passage of the blood flow) limited by the presence of a peripheral suture ring external to the prosthesis;
- impossibility of orienting the valve prosthesis by rotation once it is sutured at the corresponding anatomical structures; and
- particularly challenging implant technique, with the need for a specific apprenticeship by the operator in the case of stentless biological valves.

The object of the present invention, therefore, is to overcome the important problems associated to currently existing and clinically available heart valve prostheses.

Moreover, the structural modifications introduced by the invention, in accordance with the main aspect thereof, make the surgical procedure for the implant simpler, more precise and safer.

25 DISCLOSURE OF INVENTION

The invention relates to a heart valve prosthesis, in the current biological embodiment, but the construction of a mechanical valve prosthesis in

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accordance with the characteristics claimed in the claims is not precluded conceptually.

Therefore, a specific characteristic of the invention is to provide a modular valve prosthesis apparatus, in particular for cardiac applications, whose structural components are assembled together, in reversible fashion, by magnetic attraction with evident derived advantages.

By way of non limiting example, a possible embodiment of a biological valve prosthesis shall be illustrated below, although the concept can be extended to any type of valve prosthesis.

BRIEF DESCRIPTION OF THE DRAWINGS

The present invention shall be described in detail with reference to the accompanying drawings, which illustrate and embodiment provided purely by way of non limiting example, in which:

- Figure 1 shows a three-dimensional global view of a valve prosthesis apparatus, in particular for cardiac applications, of the present invention; in this global view, the apparatus is shown in its "closed" configuration;
- Figure 2 shows a suture ring which is a part of the apparatus of Figure 1; and
- Figure 3 shows a three-dimensional global view of a stent, which is also a part of the apparatus of Figure 1.

BEST MODE FOR CARRYING OUT THE INVENTION

For a better understanding of the terminology used in the detailed description of the present invention, a short explanation shall be provided below.

5

- Biological valve prosthesis: Substitute of a heart valve made, partially or totally, of a material of biological origin (generally, of animal origin). The most important structural components of a biological valve prosthesis are the "valve strips" made of biological material (bovine pericardium or porcine valve strips), and a "support structure" (the so-called "stent") made of plastic material; said "support structure" (stent) is not present in so-called stentless valves (without support).
- Suture ring: it is a ring made of synthetic material.

20

All these components ("valve strips", "stents", "suture ring") in traditional and known heart valve prosthesis apparatuses are assembled during their production, in such a way as to constitute a single body and no case can they be separated from each other in the subsequent steps without irreversible damaging the apparatus making it unusable for implant purposes.

As shown in the accompanying figures, a valve

prosthesis apparatus 10 comprises a valve prosthesis 20 and a suture ring 30.

In turn, the valve prosthesis 20 comprises firstly a support structure (stent) 21, derived from stent that 5 is a commonly used in the construction of biological prosthesis. The stent 21 is made of a rigid or preferably slightly flexible plastic material. Moreover, the stent 21 can be made of any other biocompatible material (steel, titanium, etc.).

10 As shown in particular in Figure 3, the stent 21 comprises an annular portion 21a and three projecting portions 21b, advantageously positioned 120° from each other. Said projecting portions 21b are obtained integral with the annular portion 21a. At the base wall 15 of the annular portion 21a, a continuous groove 21c is mechanically obtained; said groove 21c is able to house a plurality of permanent magnets 21d positioned mutually parallel.

In an embodiment not shown herein, instead of the 20 plurality of permanent magnets 21d, it is possible to provide a single permanent magnet with annular shape or another geometry.

The permanent magnets 21d used in the embodiment described herein belong to the category of magnets 25 provided with high attraction force (neodymium-iron-boron) and are coated with a material (epoxy resins or others) that is able to prevent their oxidation over time. The polarity of the magnets is oriented uniformly

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along the whole base of the stent 21 in such a way as to exert a homogeneous attraction of a corresponding structure positioned on the suture ring 30 which shall be described below.

5 The geometric shape of the base of the stent 21 is a circumference developed along a planar axis. In other embodiments, not shown herein, the geometry and the axis of the annular portion 21a of the stent 21 housing the magnets 21d can be modified.

10 The suture ring 30, in the current embodiment, exactly matches in its external and internal diameter the annular portion 21a of the stent 21. It is obtained by cutting the annular portion 21a of the stent 21 itself along a transverse axis. In this case, too, as
15 shown in particular in Figure 2, a groove 30a is obtained mechanically; the groove 30a has the exact dimensions of the groove 21c obtained in the annular portion 21a of the stent 21, in order to house a similar plurality of magnets 30b arranged parallel to each other
20 and with polarity oriented in such a way as to attract magnetically the magnets 21d positioned in the annular portion 21a of the stent 21.

Moreover, the suture ring 30 is coated by a synthetic tissue 50 for suturing the suture ring 30 to
25 intracardial anatomic structures (valve annulus) (not shown).

The valve prosthesis 20 shown in Figure 1 has three valve strips 40 which can be made of any material of

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biological or synthetic origin.

Said valve strips 40 are assembled on the stent 21 with different procedures, normally by means of manually suture when they are fabricated. The valve strips 40 can 5 also be housed within the stent 21 or be part of an integral structure "capped" outside the stent 21.

Advantageously, to obtain the valve strips 40 it is possible to use the corneal stroma of a fish, in particular of a tuna fish.

10 The surfaces of the annular portion 21a of the stent 21 and of the suture ring 30 are preferably coated with synthetic tissue 50 of such thickness as not to interfere or reduce magnetic attraction, and in such a way as not to create interruptions in the course of the 15 subsequent magnetic coupling between the two modules of the apparatus 10 constituted by the valve prosthesis 20 and by the suture ring 30.

In particular, the synthetic tissue 50 positioned at the suture ring 30 extends for a short segment in 20 order to be easily sutured to intracardiac structures (not shown).

Hereafter are described, by way of example, the standard manners of assembling the two main modules, i.e. the valve prosthesis 20 and the suture ring 30, 25 during an aortic valve replacement. It is readily apparent for those skilled in the art that the same teachings can be applied to any tubular structure of the body and in particular to any heart valve (aortic,

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mitral, tricuspid, pulmonary).

The operation is normally performed through a median sternotomy, but other manners of accessing the heart are possible, such as lateral thoracotomy or other known ones. After cannulating the cardiac and vascular structures to allow the activation of extra-body circulation, the heart is arrested by infusion of a cardioplegic solution.

With the heart motionless and bloodless, the ascending aorta is transversely sectioned for a sufficient extension to provide an ample visualisation of the aortic valve and of the aortic annulus (peripheral circular anatomical portion where the three aortic valve strips are anchored in the transition point between left ventricle and origin of the aorta artery). After conducting the exeresis of the (pathological) valve strips at the insertion of the valve annulus, by means of a suitable instrument (sizer) the exact diameter of the valve annulus is measured for the selection of the prosthetic apparatus 10 having matching dimensions.

The subsequent phase, referred in particular to the invention, consists of suturing with surgical thread the magnetic suture ring 30 (module no. 1) of the apparatus 10 at the aortic valve annulus. In this phase, particular attention is paid in orienting the face of the suture ring 30 containing the magnets distally with respect to the heart in order to be subsequently able to

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attract the valve prosthesis 20 (module no. 2) magnetically.

It is readily apparent for those skilled in the art that the operating time for suturing the suture ring 30 at the aortic valve annulus is far simpler and more rapid than the traditional technique of suturing an entire valve apparatus to the annulus in accordance with the prior art. The valve prosthesis 20 (module no. 2), also magnetic, is then approached to the suture ring 30 (module no. 1) previously fastened to the annulus, causing a mutual magnetic attraction to be exerted due, as stated, to the presence of the magnets 21d, respectively 30b correctly oriented along the entire circumferences of the modules no. 1 and no. 2 having identical diameter.

The coupling by means of magnetic force is therefore immediate, secure, without interruptions between the two modules no. 1 and no. 2, coupled and without differences in diameter between them. The modular valve prosthesis apparatus thus assembled has the advantage of the ability to orient the module no. 2 *in situ* with respect to the module no. 1 (which is fixed). This is obtained by exerting a slight force inducing the sliding along the same axis of the module no. 2 on the module no. 1, without losing magnetic contact between said modules. The possibility of rotate the valve prosthesis 20 (module no. 2) *in situ* relative to the suture ring 30 (module no. 1) is particularly

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advantageous for a correct orientation in terms of aortic flow and of the optimal perfusion of the adjacent coronary ostia. Moreover, the apparatus 10 does not have a suture ring positioned at the periphery of the base of 5 the stent, allowing the implant of a valve prosthesis with greater effective diameter than traditional apparatuses, with evident advantages of haemodynamic performance of the implant.

In an alternative embodiment (not shown herein), 10 the prosthetic apparatus can be implanted via trans-catheter, i.e. without proceeding with a traditional heart surgery operation.

In this alternative embodiment, the prosthetic apparatus comprises, as in the embodiment already 15 described above, two main modules (module no. 1 and module no. 2), i.e. a valve prosthesis (module no. 2) and a suture ring (module no. 1).

In this case, the base of the valve prosthesis (module no. 2) is no longer a rigid structure in which 20 the magnets are inserted, as in the embodiment already described above, but the magnets are sutured in the base of the biological tissue, thus allowing the possibility of temporarily reducing the diameter of the base of the valve prosthesis so it can be inserted in a catheter of 25 smaller diameter than the original diameter of the prosthesis.

The suture ring (module no. 1) in this case is also not rigid, but the magnets are assembled within a

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synthetic material (polyester) which is also thin and easily deformed.

Therefore, in this case too it is possible simultaneously to reduce the diameter of the suture ring
5 to allow its insertion in a catheter having considerably smaller diameter than the original diameter of the suture ring.

In practice, the two magnetic modules no. 1 and no. 2 are simultaneously reduced in size by compression and
10 are inserted in series into an appropriate catheter. Under constant angiographic control, the catheter carrying the modules no. 1 and no. 2 is inserted into a peripheral artery or vein (e.g. femoral artery or femoral vein).

15 Once the heart is reached (in particular the site of the implant, aortic, pulmonary, mitral, tricuspid valve) the suture ring is released and expanded (with a balloon comprised in the catheter system) until it assumes its original diameter. Said suture ring is
20 secured at the implant site (valve annulus).

The anchoring of the magnetic suture ring can be facilitated by the presence of hooks situated at the outer circumference of the module no. 1.

Immediately thereafter, the actual valve prosthesis
25 is released. It is also expanded with a balloon comprised in the catheter system, returning to its original diameter, which exactly matches the diameter of the suture ring. By magnetic attraction, the two modules

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no. 1 and no. 2 are coupled in a manner that is exactly similar to the one described in relation to the first embodiment for which, as stated, a traditional surgical technique is used.

5 To summarise, the advantages of the valve prosthesis apparatus of the present invention are the following:

- (a) it can be implanted with an extremely simple, rapid and reliable technique;
- 10 (b) it can be replaced in case of need with a particularly simplified surgical procedure, in short operating times and with reduced risk for the patient;
- (c) it can be rotated, in extremely simple and non traumatic fashion, *in situ* (after the implant) for a correct anatomical orientation;
- 15 (d) it assures better haemodynamic performance (corresponding to a greater effective area of the valve orifice) than existing prostheses;
- (e) the capability of replacing the valve prosthesis (in particular, module no. 2, bearing the valve strips 40 which are normally subject to structural deterioration) without having to perform the exeresis of the suture ring (module no. 1) from the native valve annulus; to replace the module no. 2 leaving the module no. 1 *in situ*, it is

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sufficient to exert a force contrary to the magnetic attraction between two modules able to induce their separation (disassembly); it is evident that the operating phase necessary for the exeresis of the suture ring of a prosthesis from the heart and the suture of a new prosthesis entails more prolonged times, greater risks and likelihood of errors with respect to the mere replacement of the module no. 2 at the module no. 1 by simple and very rapid magnetic attraction; and

- (f) the execution of the intervention to implant the valve prosthesis apparatus via trans-catheter allows considerable advantages for the operated patients; said implant technique does not require surgical access to the heart by means of sternotomy or thoracotomy, and it is not necessary to open the cardiac cavities, so it is not necessary to provide an implant which achieves an extra-body circulation; furthermore, an additional evident advantage of the trans-catheter implant is that it assures far more rapid recovery times than the traditional one.

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CLAIMS

1. A valve prosthesis apparatus, in particular for cardiac applications, apparatus (10) comprising a valve prosthesis (20) applied on a suture ring (30); apparatus (10) that is characterised in that said valve prosthesis (20) is fastened to said suture ring (30) by magnetic means (21d, 30b).
- 10 2. Valve prosthesis apparatus (10) as claimed in claim 1, characterised in that said magnetic means (21d, 30b) are contained in a respective continuous groove (21c, 30a) obtained respectively on said valve prosthesis (20) and on said suture ring (30).
- 15 3. Apparatus (10) as claimed in claim 2, characterised in that at least one part of said magnetic means (21d) are contained in a continuous groove (21c, 30a) obtained in a stent (21), which is a part of said valve prosthesis (20).
- 20 4. Apparatus (10) as claimed in either of the claims 2 or 3, characterised in that said magnetic means (21d, 30b) comprise a plurality of magnets (21d, 30b).
- 25 5. Apparatus (10) as claimed in either of the claims 2 or 3, characterised in that said magnetic means (21d, 30b) comprise magnets with annular shape.

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6. Apparatus (10) as claimed in any of the previous claims, characterised in that said valve prosthesis (20) comprises a stent (21) and valve strips (40).

5 7. Apparatus (10) as claimed in claim 6, characterised in that said valve strips (40) are made of a biomaterial.

8. Apparatus (10) as claimed in claim 7, characterised 10 in that said biomaterial is derived from corneal stroma, in particular from corneal stroma of tuna fish.

9. Apparatus (10) as claimed in any of the previous claims, characterised in that at least one portion of 15 said valve prosthesis (20) and at least one portion of said suture ring (30) are coated by a synthetic tissue (50) able to facilitate the suture of said valve prosthesis (20) and of said suture ring (30).

20 10. Apparatus (10) as claimed in claim 1, characterised in that said valve prosthesis and said suture ring are made of deformable materials such as to allow their insertion into the body of a patient through a catheter, i.e. without having to proceed to a traditional heart 25 surgery operation.

11. Apparatus (10) as claimed in claim 10, characterised in that the magnets are immersed in said

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deformable materials.

12. Apparatus (10) as claimed in either of the claims 10 or 11, characterised in that the suture ring is made 5 of a synthetic material, in particular polyester.

13. Apparatus (10) as claimed in any of the claims 10, 11, 12, characterised in that the suture ring has a plurality of hooks able to facilitate its fastening in 10 the implant site.

14. A system for implanting in the human body a prosthetic apparatus comprising a magnetic valve prosthesis and a magnetic suture ring which are easily 15 deformable by compression; said implant system comprising the following steps:

- (a) temporarily reducing by compression the dimensions of the magnetic valve prosthesis (module no. 2) and the magnetic suture ring (module no. 1) in such a way as to allow their insertion in a catheter able 20 to transport said modules no. 1 and no. 2 in the implant site;
- (b) inserting said catheter carrying said modules no. 1 and no. 2 into a peripheral vein or artery under 25 constant angiographic control;
- (c) releasing the suture ring, which is expanded until assuming the original dimensions, once it reaches the implant site;

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- (d) fastening said suture ring in the implant site;
- (e) releasing the valve prosthesis, which is expanded until assuming the original dimensions, once it reaches the implant site; and
- 5 (f) magnetically fastening said valve prosthesis to said suture ring.

1 / 1

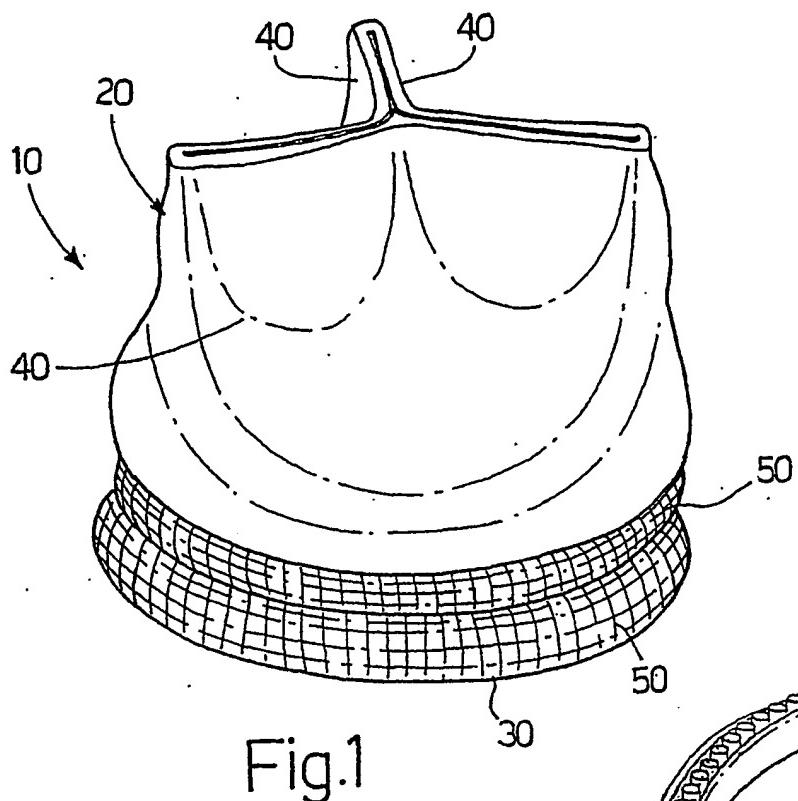


Fig.1

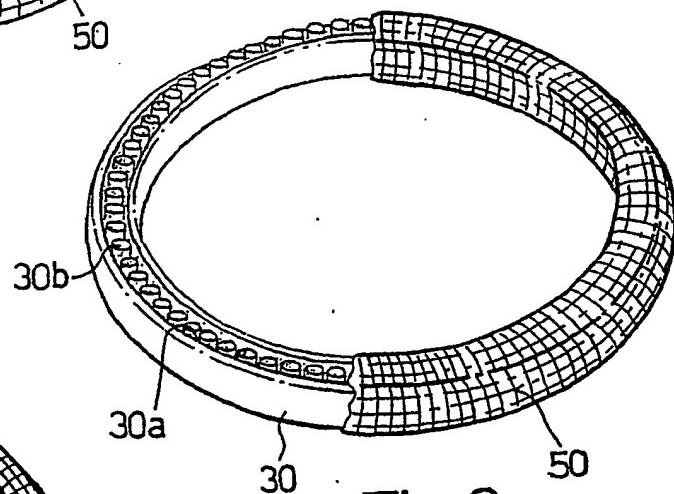


Fig.2

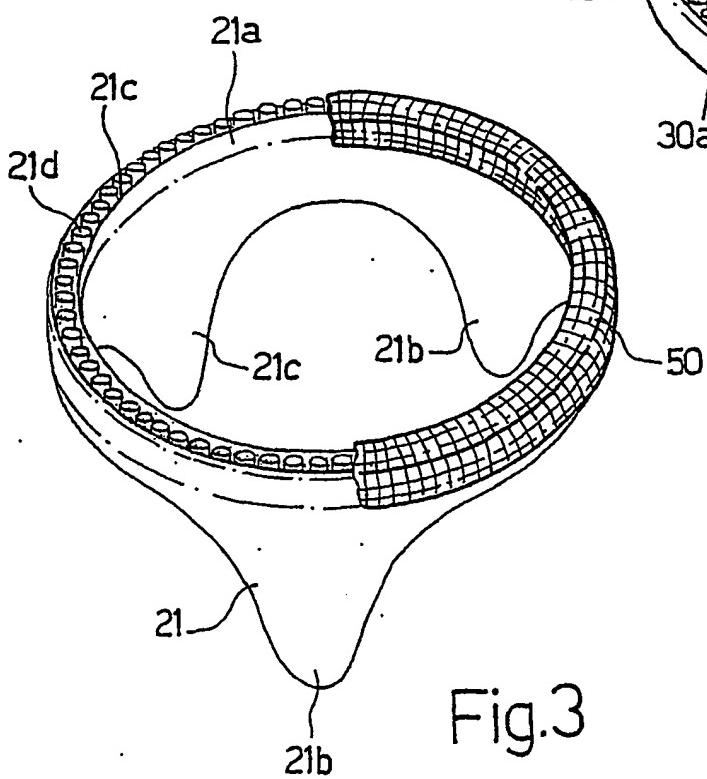


Fig.3

A. CLASSIFICATION OF SUBJECT MATTER
IPC 7 A61F2/24

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC 7 A61F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
P,X	WO 2004/058106 A (ARBOR SURGICAL TECHNOLOGIES, INC; FOGARTY, THOMAS, J; DREWS, MICHAEL,) 15 July 2004 (2004-07-15) paragraph '0070! - paragraph '0075! paragraph '0121! claim 70 figures 11-15	1,6,7, 9-12
A	US 5 571 175 A (VANNEY ET AL) 5 November 1996 (1996-11-05) column 3, line 59 - column 4, line 5 column 8, line 17 - line 20	1-13
P,A	US 6 652 540 B1 (COLE DAVID H ET AL) 25 November 2003 (2003-11-25) column 4, line 66 - column 13, line 3	1-13

Further documents are listed in the continuation of box C.

Patent family members are listed in annex.

* Special categories of cited documents:

- *A* document defining the general state of the art which is not considered to be of particular relevance
- *E* earlier document but published on or after the international filing date
- *L* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- *O* document referring to an oral disclosure, use, exhibition or other means
- *P* document published prior to the international filing date but later than the priority date claimed

T later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

X document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

Y document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.

& document member of the same patent family

Date of the actual completion of the international search

Date of mailing of the international search report

8 February 2005

17/02/2005

Name and mailing address of the ISA

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Mary, C

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	CH 608 368 A5 (SULZER AG) 15 January 1979 (1979-01-15) column 1, line 15 - column 2, line 67 -----	1-13
A	US 5 123 918 A (PERRIER ET AL) 23 June 1992 (1992-06-23) column 8, line 22 - column 13, line 5 -----	1-13

INTERNATIONAL SEARCH REPORT

International application No.
PCT/IB2004/003480

Box II Observations where certain claims were found unsearchable (Continuation of item 2 of first sheet)

This International Search Report has not been established in respect of certain claims under Article 17(2)(a) for the following reasons:

1. Claims Nos.: 14 because they relate to subject matter not required to be searched by this Authority, namely:
Rule 39.1(iv) PCT - Method for treatment of the human or animal body by surgery
2. Claims Nos.: because they relate to parts of the International Application that do not comply with the prescribed requirements to such an extent that no meaningful International Search can be carried out, specifically:
3. Claims Nos.: because they are dependent claims and are not drafted in accordance with the second and third sentences of Rule 6.4(a).

Box III Observations where unity of invention is lacking (Continuation of item 3 of first sheet)

This International Searching Authority found multiple inventions in this international application, as follows:

1. As all required additional search fees were timely paid by the applicant, this International Search Report covers all searchable claims.
2. As all searchable claims could be searched without effort justifying an additional fee, this Authority did not invite payment of any additional fee.
3. As only some of the required additional search fees were timely paid by the applicant, this International Search Report covers only those claims for which fees were paid, specifically claims Nos.:
4. No required additional search fees were timely paid by the applicant. Consequently, this International Search Report is restricted to the invention first mentioned in the claims; it is covered by claims Nos.:

Remark on Protest

- The additional search fees were accompanied by the applicant's protest.
- No protest accompanied the payment of additional search fees.

Patent document cited in search report		Publication date		Patent family member(s)		Publication date
WO 2004058106	A	15-07-2004	US	2004122516 A1		24-06-2004
			WO	2004058106 A2		15-07-2004
			US	2004122514 A1		24-06-2004
US 5571175	A	05-11-1996	AU	6379796 A		30-12-1996
			WO	9640009 A1		19-12-1996
			US	5843179 A		01-12-1998
			ZA	9604886 A		11-02-1997
US 6652540	B1	25-11-2003	US	6352543 B1		05-03-2002
			AU	5740901 A		12-11-2001
			CA	2387618 A1		28-11-2001
			EP	1284660 A1		26-02-2003
			JP	2003533251 T		11-11-2003
			WO	0182803 A1		08-11-2001
			US	2002103495 A1		01-08-2002
			US	2004034377 A1		19-02-2004
			US	2004116945 A1		17-06-2004
			US	6719768 B1		13-04-2004
			US	2005021059 A1		27-01-2005
			US	6802847 B1		12-10-2004
			AU	755190 B2		05-12-2002
			AU	2674699 A		30-08-1999
			CA	2320956 A1		19-08-1999
			EP	1054641 A1		29-11-2000
			JP	2002502663 T		29-01-2002
			US	2003158573 A1		21-08-2003
			WO	9940868 A1		19-08-1999
			US	2002077566 A1		20-06-2002
			US	2002161424 A1		31-10-2002
			US	2001041902 A1		15-11-2001
			US	2002144696 A1		10-10-2002
			US	2004077987 A1		22-04-2004
			US	2004168691 A1		02-09-2004
			US	2004167444 A1		26-08-2004
			US	2001025643 A1		04-10-2001
CH 608368	A5	15-01-1979		NONE		
US 5123918	A	23-06-1992	FR	2642960 A1		17-08-1990
			AT	91613 T		15-08-1993
			DE	69002254 D1		26-08-1993
			DE	69002254 T2		03-02-1994
			DE	383676 T1		07-02-1991
			EP	0383676 A1		22-08-1990
			ES	2017595 T3		01-01-1994
			JP	1883541 C		10-11-1994
			JP	3103253 A		30-04-1991
			JP	6004081 B		19-01-1994